

# Development of visible and NIR imaging equipment for small animals with smart pad

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**Abstract.** The portable visible and near-infrared (NIR) imaging equipment for a pre-clinical test with small animals was designed and developed in this paper. The developed equipment is composed of a CCD camera, a focusing lens, an objective lens, a NIR band pass filter and a NIR filter driving motor. An NIR ray is mainly used for imaging equipment because it has high light penetration depth in biological tissue. Therefore, NIR fluorescent agents are available for chemical conjugation to targeting molecules in vivo. This equipment can provide a visible image, NIR image and merged image simultaneously. A communication system was specifically established to check obtained images through a smart pad in real time. It is less dependent on space and time than the conventional system.

**Keywords:** Visible/NIR image, animal imaging, fluorescence, mobile-based, merged image

## 1. Introduction

Development processes (new drug, biomarker, etc.) need too much money and a long time. Pre-clinical tests are required to verify the effectiveness of new drugs or bio-markers [1,2]. In the process of a preclinical test, researchers normally use imaging equipment with small animals. This equipment provides biological imaging of biotransformation to researchers.

There are many types of imaging equipment such as optical imaging, nuclear imaging, magnetic resonance imaging, ultrasonic imaging, photo-acoustic imaging and Raman spectroscopic imaging. Imaging equipment has its advantages and disadvantages respectively. Nuclear imaging systems have high sensitivity, but low resolution. In addition, using radioactivity has legal restrictions. In the case of magnetic resonance imaging systems, they have high resolution, but low sensitivity. Optical imaging systems have superior sensitivity and provide imaging faster than other imaging systems [3]. Because of its advantages, many researchers use optical imaging systems when undergoing pre-clinical tests. These imaging techniques are differently used to diagnosis a certain disease because imaging systems

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have different spectrums. Multi-imaging equipment is developed as combining different imaging systems nowadays [4].

NIR wavelength range is from 700nm to 1000nm. The use of NIR light for biomedical imaging is grounded in first principles and is best understood in the context of photon propagation through living tissue and the signal to noise ratio. Generally, the photon absorbance of a particular tissue or organ is all-absorbing components. In living, non-pigmented tissue, the major NIR absorbers are water, lipids and hemoglobin. In a typical tissue, having 8% blood volume and 29% lipid content, the dominant absorber is hemoglobin, accounting for 39~63% of the total absorbance at NIR wavelengths [5].

In order to develop imaging equipment, the researchers have to consider fluorescent agents properties, tissue targeting and selectivity of emitted fluorescent agents etc. In this study, new imaging equipment using visible ray and near-infrared ray for pre-clinical tests with small animals was developed. This equipment can provide a visible image, NIR image emitting fluorescent agents and a merged image simultaneously. It helps the researcher to understand visible messages. A communication system was specifically established to check obtained images through a smart pad in real time. Also, this equipment was made portable to move easily.

## 2. Experimental

### 2.1. Design of the visible and NIR imaging equipment for small animals

The schematic diagram of equipment is shown in Figure 1. In this equipment, a CCD camera was used to take visible and NIR images. A focusing lens and an objective lens are installed under a CCD camera. In order to pass only NIR light source, a NIR band pass filter was used, which is equipped with an automatic driving motor. There are NIR light sources for fluorescent agents around an object bed and visible light sources for illuminating an object under a ceiling. An object bed can move up and down with z-axis stepping motor (Figure 1).

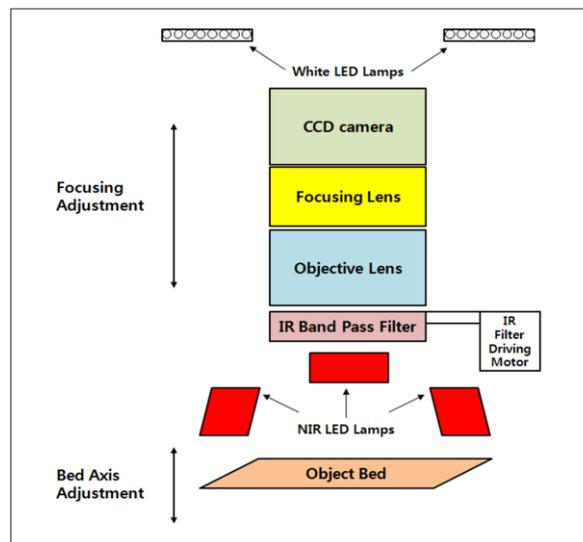


Fig. 1. Schematic diagram of portable visible and NIR imaging equipment.

In the optical system, a CCD camera has a pixel size of  $4.40 \times 4.40 \mu\text{m}$  and the resolution is 1800 (H)  $\times$  1200 (V) pixels (Figure 2(a)). The focal distance of the lens is from 8 mm to 80 mm, and the zoom ratio is 10 (Figure 2(b)). IR band pass filter receives 850 nm wavelengths (Figure 2(c)). The white LEDs were used for a visible light source (Figure 2(d)), and an NIR light source emitting 750 nm wavelength for a NIR light source (Figure 2(e)). Each light source is fixed to a fabricated jig and light on the subject. Light sources are used to emit light of two wavelengths simultaneously or selectively.

To observe visible and NIR images, an imaging program was developed. Obtained images are shown on the computer screen through the imaging program. There are still cut images, visible images, NIR images and merged images on one screen. A merged image is an overlapped image of visible and NIR. It will be helpful for a researcher to understand visible messages.

### *2.2. Preparation of the PLGA/HSA/ICG nanoparticles for NIR images*

In this study, nanoparticles were prepared by following the double emulsion method [6,7]. The nanoparticles are used by using the NIR image using the equipment. ICG as NIR fluorescent agents was encapsulated into the PLGA by using the double emulsion method. The PLGA is a biocompatible and biodegradable polymer that was approved by the Food Drug Administration (FDA). A preparation scheme of nanoparticles is shown in Figure 3.

In a double emulsion (W1/O/W2) method, PLGA (100 mg) were dissolved in methylene chloride (2 ml). ICG (5 mg) and HSA (15 mg) were dissolved in water (250 ml). An aqueous solution containing ICG-HSA complex was emulsified in PLGA solution by the high-speed homogenizer for 5 min. The resulting primary emulsion was added to PVA (4%, w/w; 30 ml) and emulsified using micro-tip probe sonicator (CV18, 700W, 20 kHz, SONICS&MATERIALS, USA) set 90% power for 5 min. The resultant double emulsion was agitated with a magnetic stirrer overnight at room temperature until the evaporation of methylene chloride was complete. The PLGA/HSA/ICG nanoparticles were collected by ultracentrifugation (17,000 rpm, 10 min), washed three times with distilled water, freeze-dried, and stored at 4°C before use.

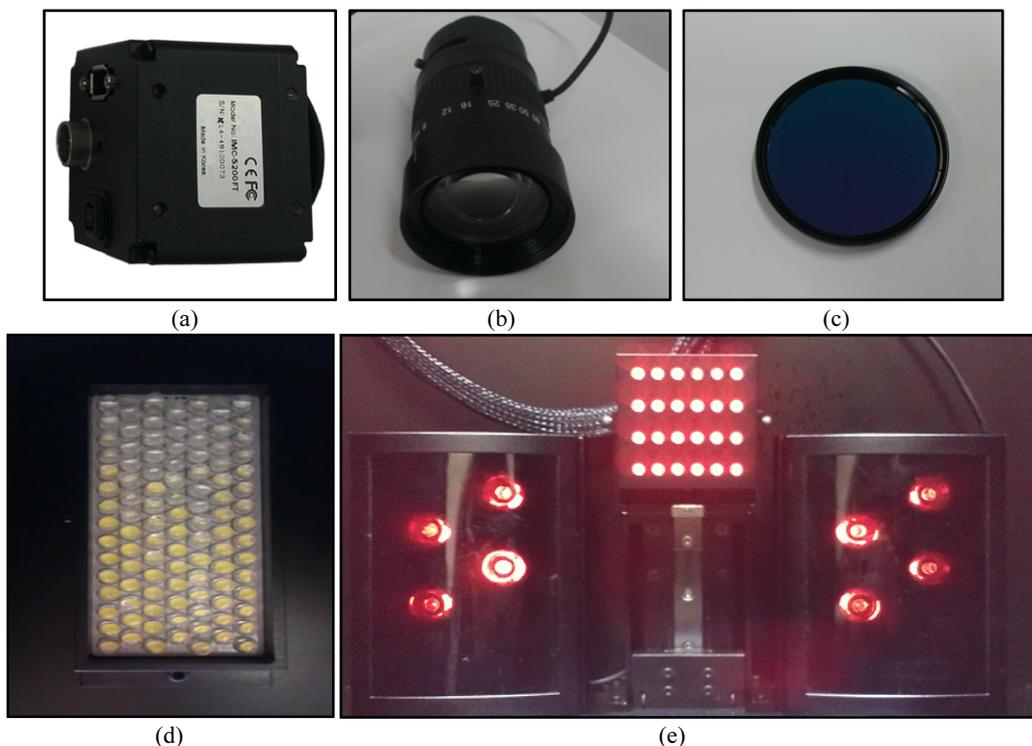
### *2.3. Characterization of the PLGA/HSA/ICG nanoparticles*

The morphology of the PLGA/HSA/ICG nanoparticles was obtained by using a field-emission scanning electron microscopy (SEM; S-4300, Hitachi, Japan). Dynamic light scattering particle size analyzer (N5, Beckman Coulter) was used to measure average diameter of the PLGA/HSA/ICG nanoparticles. The fluorescence property of the PLGA/HSA/ICG nanoparticles and ICG was measured by using a luminescence spectrometer (LS45, Perkin-Elmer, USA). The emission of PLGA/HSA/ICG nanoparticles and ICG were measured at 780 nm.

### *2.4. Observation of visible and NIR images*

In order to observe images, PLGA/HSA/ICG nanoparticles (5 mg) in PBS buffer (pH 7.4, 1.5 ml) and distilled water were prepared in Eppendorf tubes respectively. For animal testing, PLGA/HSA/ICG nanoparticles (0.5 mg) in PBS buffer (pH 7.4, 1.5 ml) were prepared. Korea Research Institute of Bioscience and Biotechnology (KRIBB) were asked to conduct animal testing. An Eight-week-old male hairless mouse (Orient Bio, Seongnam, Korea, 31.8 g) were anesthetized by Zoletil 50 (Virvabac, France, 0.08 ml/kg) of 0.025 ml through an intramuscular injection. In vivo behavior

of the PLGA/HSA/ICG nanoparticles can be observed from real-time imaging after a subcutaneous injection to a tail of a mouse.



Animal care and all experiments were conducted in accordance with KRIBB Guidelines for the Care and Use of Laboratory Animals, and all experiments were approved by the institutional review board (KRIBB Institutional animal care and use committee/KRIBB-IACUC).

### 3. Results

#### 3.1. Visible and NIR imaging equipment for small animals

The visible and NIR imaging equipment for small animals is shown in Figure 4(a). Outer size of the equipment is  $W380 \times D720 \times H420$ , and the inner size is  $W300 \times D370 \times H330$ . Also, the size of an object bed is  $W200 \times H200 \times T2$ . The object bed can move up and down with z-axis stepping motor. The weight of the equipment is 45 kg. The equipment inside is shown in Figure 4(b). A CCD camera is fixed to observe the center of an object bed. A focusing lens and an objective lens are installed to adjust the image. There are NIR light sources around an object bed and visible light sources under the ceiling. In order to pass only NIR light sources, a NIR band pass filter was used, which is equipped with an automatic driving motor. It is convenient that an object bed can move up and down using a computer system.

A camera is possible to communicate with a laptop computer using 1394A port. A laptop computer is connected to 1394A 4pin ports. In that case, it can directly be connected to the camera. A laptop computer having no connection ports is used after installing IEEE 1394PCMCIA card.

A visible image, NIR image, merged image and a still cut image were obtained simultaneously. Especially, the NIR image was taken according to control the NIR band pass filter. Each image is displayed on the screen respectively, and a full screen is available for use. There are still cut images (Figure 5(a)), visible images (Figure 5(b)), NIR images (Figure 5(c)) and merged images (Figure 5(d)) on the screen. Also, the imaging program was developed to increase sensitivity. The imaging program can adjust the exposure time and the gain value of a CCD camera.

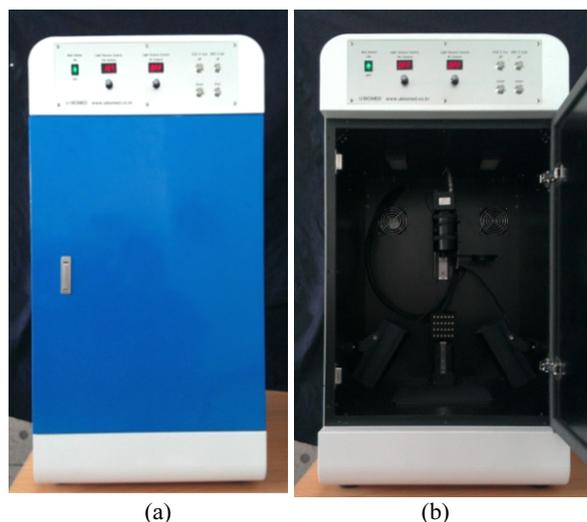


Fig. 4. Portable Visible and NIR imaging equipment (a) Outline of equipment (b) Configuration of system inside.

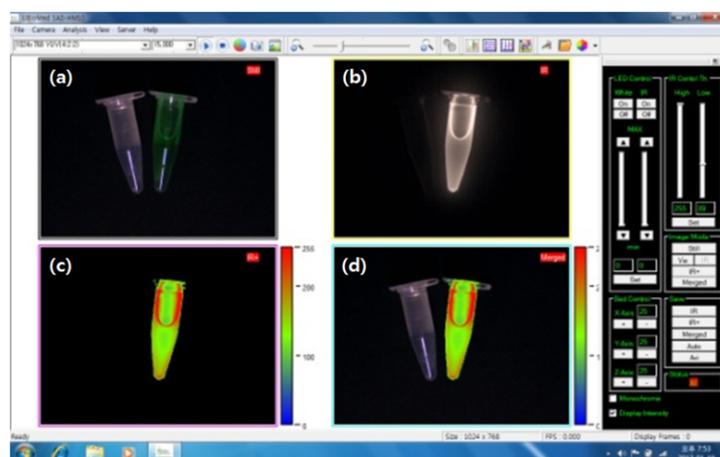


Fig. 5. Imaging viewer for Visible, NIR, and Merged image.

The resolution was set properly to a laptop computer on  $1024 \times 768$  considering the laboratory environment and user convenience. Also, there are no restrictions to adjust the resolution on the imaging program. The imaging program will automatically save the data undergoing experiments to prevent data loss. It has an additional function that images for transmission can be automatically saved and deleted. Images can be sent to homepage servers to monitor the experiment remotely.

### 3.2. Characterization of the PLGA/HSA/ICG nanoparticles

The morphology of the PLGA/HSA/ICG nanoparticles is shown in Figure 6 using a field-emission scanning electron microscopy (SEM; S-4300, Hitachi, Japan). The PLGA/HSA/ICG nanoparticles have sphere morphology. The average diameter of the PLGA/HSA/ICG nanoparticles is approximately 184 nm. ICG have emission peak at a wavelength of 820 nm and emission peak of the PLGA/HSA/ICG nanoparticles was observed at 810 nm (Figure 7).

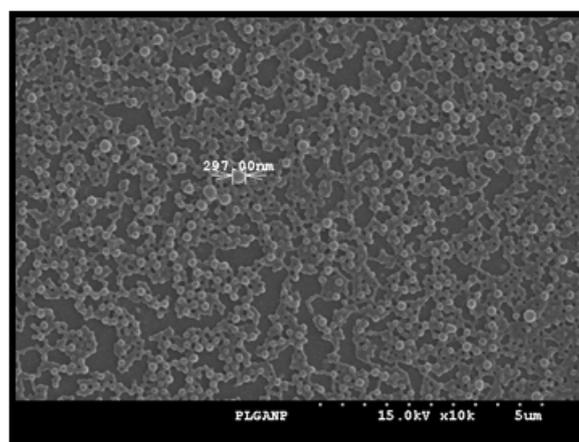


Fig. 6. SEM image of PLGA/HSA/ICG nanoparticles.

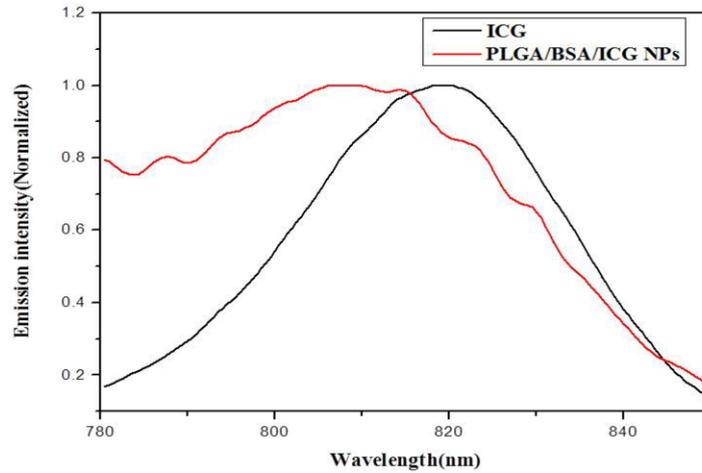


Fig. 7. Emission spectra of ICG and PLGA/HSA/ICG nanoparticles.

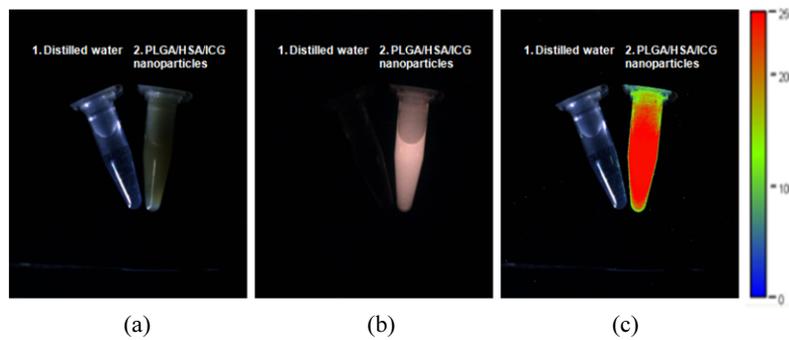


Fig. 8. Images of distilled water (left) and PLGA/HSA/ICG nanoparticles solution (right) (a) Color image (b) NIR image, and (c) Merged image.

### 3.3. Observation of visible and NIR images

The PLGA/HSA/ICG nanoparticles solution and distilled water in Eppendorf tubes respectively were prepared on an object bed and observed by using the visible and NIR imaging program as shown in Figure 8. We adjusted the value of the CCD camera through the developed imaging program. Exposure time was 1.7 seconds and gain value was 150.

Figure 8(c) shows that the merged image shows intensity of the PLGA/HSA/ICG nanoparticles with color. The color change indicates emission change of the PLGA/HSA/ICG nanoparticles.

A mouse was fixed on an object bed and observed by using the visible and NIR imaging program as shown in Figure 9. The images can observe real-time distribution of the PLGA/HSA/ICG nanoparticles after a subcutaneous injection in the tail of a mouse. These images mean a dispersion of nanoparticles and release ICG from the PLGA/HSA/ICG nanoparticles (Vishal et al., 2009). Exposure time was 3.5 seconds and gain value was 150.

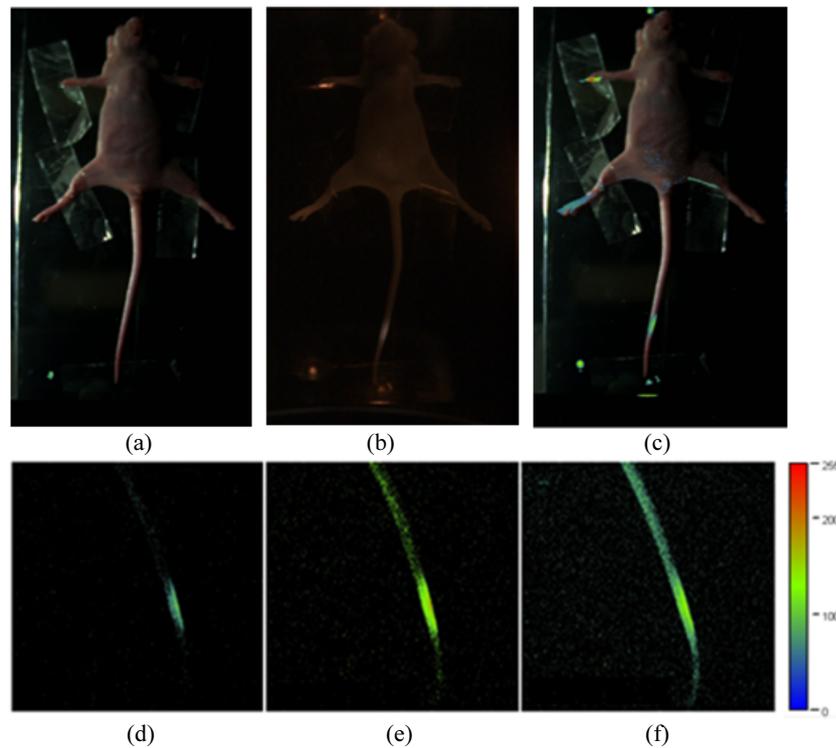


Fig. 9. Image of PLGA/HSA/ICG nanoparticles by tail subcutaneous injection of hairless mouse; (a) Color image (b) NIR image (c) Merged image (d) 5min after injection (e) 30min after injection (f) 60min after injection.

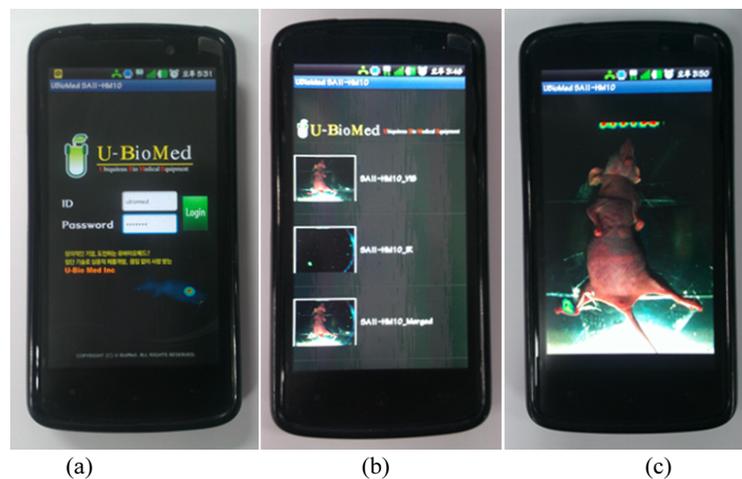


Fig. 10. Images through a smart phone application; (a) Login screen of the application (b) Screen of an imaging test using the application (c) Screen of the merged image.

Figure 9(a) is a color image, Figure 9(b) is a NIR image and Figure 9(c) is a merged image of the above two images. Figure 9(d) is a merged image after injecting the PLGA/HSA/ICG nanoparticles.

Figure 9(e) is 30 minutes after injection and Figure 9(f) is 60 minutes after injection. As a result, it is possible to track in vivo behavior of PLGA/HSA/ICG nanoparticles using this equipment.

Finally, obtained visible and NIR images were observed by using a smartphone (LG-SU640, LG, Korea) through the application program. The figure running the application program is shown in Figure 10(a). In the Figure 10(b), visible, NIR and merged image can be observed on one screen. Figure 10(c) is a zoom in the image after selecting the merged image.

#### 4. Conclusion

In this study, a portable visible and NIR imaging equipment was developed for pre-clinical tests with small animals. The advantage of the equipment is its ability to communicate with researchers who are a long distance away. To be specific, the experimental information can be shared by smart phones in real time. Therefore, researchers can save time and money when conducting a pre-clinical test. As visible light sources and NIR light sources are harmless to humans, the equipment has great potential and application ranges which can be gradually expanded.

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